

In-vitro Fatigue Resistance of Bonded Posterior Occlusal Veneers: A Systematic Review

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Abstract

Objectives: To determine the fatigue resistance of occlusal veneers and whether it can be a successful mean of restoring erosive or attrite posterior teeth. **Methods:** Search was made in 2 databases including PubMed and LILACS, the terms “occlusal veneers”, “table tops”, “overlays”, “non retentive all ceramic full coverage restorations”, “fatigue resistance”, “masticatory fatigue”, “stresses”, “fatigue failure” and “fracture strength” were used, title and abstract were screened; giving the exclusion and inclusion standards articles which did not follow the inclusion standards were excluded. Incorporated papers are then read thoroughly for a second stage filter, this was followed by manual searching. **Findings:** The search resulted in 6 included papers, 3 papers regarding the fatigue resistance of occlusal veneers made of composite and glass ceramic blocks, 1 paper measuring the fatigue resistance of occlusal veneers made of two different glass ceramics, 1 paper comparing occlusal veneers made of resin nano-ceramic with those made of composite blocks and 1 paper simulating five years of clinical service on occlusal veneers made of one type of glass ceramic. From the included studies occlusal veneers were found to be a successful mean of restoring erosive or attrite posterior teeth regarding fatigue resistance.

Keywords: Composite and Resin Nano-Ceramic, Fatigue Resistance, Glass Ceramics, Occlusal Veneers

1. Introduction

An ultimate restorative material must fulfill functional and esthetic desires. It has to also offer continuing reliability in addition to teeth preservation¹⁻³.

Through enhancements in the biocompatibility, esthetics and the mechanical properties of ceramics, the use of all-ceramics with metallic restorations is defensible². Production methods such as heat press or CAD/CAM (computer assisted design/computer-assisted machining) procedures are used to manufacture also inlays or onlays (small all-ceramic restorations) with high fracture resistance⁴.

With huge carious defects, many studies have well documented the worthy durability of ceramic onlays⁵⁻⁷ and crowns^{8,9}.

With mal positioned teeth or occlusal abrasion with no caries occlusal restorations is essential. Orthodox treatments were partial crown preparations or retentive inlay^{10,11}. Though, a less aggressive non-retentive

preparation design is promising when adhesive cementing methods are used¹².

Progressive reduction of enamel breadth is a biological state as a result of aging¹³. Though, the accelerated and premature enamel loss by Gastro Esophageal Reflux Disease (GERD) or bulimia nervosa can happen in childhood or adolescence, with damaging costs^{14,15}. On the other hand, as mineral loss is sluggish, slow and usually trouble-free, dental erosion is frequently overlooked. It is usually diagnosed at a progressive stage, once a significant loss of enamel has arisen^{15,18}.

The management of dental erosion must be concentrated on the cause and inhibition of additional damage, the restorative phase needs a cautious method, dependent on the grade of destruction¹⁵.

Initial lesions require simply a clinical follow-up, non-invasive dentin sealing with a bonding agent, or direct composite resin restorations. Nevertheless, management of patients with wear and generalized erosion is further multifaceted¹⁵.

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In-vitro tests have boundaries and do not essentially determine the clinical success of all-ceramics; though, they signify the greatest obtainable information about dental restorations. In-vivo data has been inadequate until now due to ethical and practical reasons. Thus, this review will concentrate on systematically evaluating the fatigue resistance of occlusal veneers made of different materials.

2. Materials and Methods

The PRISMA (Preferred Reporting Items for Systematic Reviews and Meta-Analyses) statement¹⁹ was followed as much as possible.

2.1 Data Collection

Two online databases were systematically searched: PubMed (NLM—National Library of Medicine) and LILACS (Virtual Health Library). The search terms “occlusal veneers”, “table tops”, “overlays”, “non retentive all ceramic full coverage restorations”, “fatigue resistance”, “masticator fatigue”, “stresses”, “fatigue failure” and “fracture strength” were used to search in vitro studies up to December 2015. The electronic search was not restricted. The last search strategy was tweaked using the help of a librarian.

2.2 Criteria for Inclusion of Studies

From the search outcomes according to titles/abstracts related to topic, studies were nominated founded on these inclusion standards:

Inclusion:

- Occlusal veneers
- In-vitro studies

A complete copy of a study was evaluated for inclusion, when a related title with no abstract was available, as explained below. Two independent reviewers assessed the studies’ titles and abstracts of possible studies. All abstracts that seemed to meet inclusion criteria were chosen and full articles or full theses were acquired. Manual search was used to complete the literature search within the reference lists of nominated full-text studies. Only articles that met with the inclusion standards were additionally reviewed. Two reviewers reviewed independently full copies of articles to decide if the exclusion standards applied. Besides the preliminary selection the subsequent exclusion standards were only considered at this stage:

- Onlays.
- Inlays.
- Endodontically treated teeth.

2.3 Data Extraction

The materials were extracted shown in Table 1, the experimental conditions shown in Table 2, as were the results shown in Table 3. For any incomplete/missing information, the articles’ authors were communicated. Evaluation of study risk of bias was conducted with individual information collected in Tables.

Table 1. Materials

Paper title	Materials							
	Extracted molars	Finite element	CAD/CAM			Heat pressed		
			Empress	e.max	Composite	Empress	e.max	
Clausen et al ¹² in 2010	64						√	√
Magne P. et al ²⁰ in 2010	30		√	√	Paradigm MZ 100			
Schlichting et al ²¹ in 2011	40		√	√	Paradigm MZ 100 and XR			
Magne p. et al ²² in 2012		√	√	√	Paradigm MZ 100			
Skouridou N et al ²³ in 2013	10		√					
Johnson AC et al ²⁴ in 2014	60			Lava Ultimate	Paradigm MZ 100			

Table 2. Methodology

Paper title	Preparation		Thickness of Occlusal veneers	surface treatment			Cementation	Tests
	beveled F.L.	Chamfer F.L.		Ceramics	Composite	Preparation		
Clausen et al ¹² in 2010	√	√ (0.8mm)	1.5 mm	HF etched and silanated		Etched and primer applied	adhesive resin cement (Variolink II)	Cyclic loaded 600,000 times and thermocycled 3500 times in a masticatory simulator. Surviving specimens were loaded until, fracture in a universal testing machine
and the preparation was either completely within Enamel or within Dentin								
Magne P. et al ²⁰ in 2010	√		1.2 mm	HF etched and silanated	airborne-particle abraded and silanated	airborne-particle abraded, etched and adhesive resin applied	Preheated adhesive resin cement (Filtek Z100)	Cyclic loading at 200N, followed by of 400, 600, 800, 1000, 1200 and 1,400N at a maximum of 30,000 cycles each.
Schlichting et al. ²¹ in 2011	√		0.6 mm	HF etched and silanated	airborne-particle abraded and silanated	airborne-particle abraded, etched and adhesive resin applied	Preheated adhesive resin cement (Filtek Z100)	Cyclic loading at 200N, followed by of 400, 600, 800, 1000, 1200 and 1,400 N at a maximum of 30,000 cycles each.
Magne p. et al. ²² in 2012	√		0.6 mm					Nonlinear contact analysis at 200N and 800 N.
Skouridou N et al. ²³ in 2013		√ 0.5 mm		HF etched and silanated		Etched and adhesive resin applied	adhesive resin cement (Variolink II)	thermal cycling and mechanical loading in a masticatory simulator
Johnson AC et al. ²⁴ in 2014	√		0.3, 0.6 and 1 mm	airborne-particle abraded		etched	self-adhesive, dual-cure resin cement (RelyX Unicem)	Each specimen was subjected to vertical load to fracture using a universal testing machine

3. Results

Six studies^{12,20-24} were incorporated in the systematic review shown in Figure 1. After inclusion and exclusion standards were used in the second selection stage,

two studies were excluded. The designated studies were published between 2010 and 2014. They varied extensively in the methodology, and study design (specimens count and materials used). So the opportunity of attempting a meta-analysis was precluded.

Table 3. Results

Paper title	Results
Clausen et al ¹² in 2010	All specimens survived the masticatory fatigue. Mean fracture resistance ranged from 2895 to 4173N. Influence of ceramic material on fracture resistance was significant ($p = 0.0001$). Lithium disilicate glass-ceramic restorations had higher fracture resistances than leucite reinforced glass-ceramic restorations. Different preparation designs showed no significant influence on fracture resistance ($p = 0.0969$). The design of the finishing line did not influence the fracture resistance ($p = 0.9461$)
Magne P. et al ²⁰ in 2010	For the IPS Empress group, restorations demonstrated failure at an average load of 900 N (110,918 cycles), and all specimens exhibited ceramic cracks by the completion of the 185,000 cycles (survival=0%). For groups EMAX and MZ100, the survival rates (no cracking) were 30% and 100%, respectively
Schlichting et al ²¹ in 2011	In the IPS Empress group, restorations failed (initial failure) at an average load of 500N (38,475 cycles), in group e.max at an average load of 800N (87,089 cycles) and none of the specimens withstood all 185,000 load cycles (survival = 0% for both ECAD and EMAX). For groups MZ100 and XR the survival rate was 60% and 100%, Respectively
Magne p. et al ²² in 2012	none of the Empress CAD and only 20% of the e.max CAD occlusal veneers survived the load of 800N at 0.6 mm thickness (average failure load of 800N), group MZ100 did not fail in 90% of the specimens
Skouridou N et al ²³ in 2013	The occlusal veneers (Group III) developed surface cracks or fractures during thermocycling and mechanical loading and therefore excluded from fracture strength testing
Johnson AC et al ²⁴ in 2014	Mean maximum loads (N)at the point of fracture for the MZ groups were 1620 (MZ3), 1830 (MZ2), and 2027 (MZ1) for the material thicknesses of 0.3, 0.6, and 1.0 mm, respectively. The Lava Ultimate (LU) groups fractured at slightly higher average loads (N) of 2078 (LU3), 2141 (LU2), and 2115 (LU1) at the respective 0.3, 0.6, and 1.0 mm thicknesses

3.1 Results of Individual Studies

- Study design: five studies were in-vitro^{12,20,21,23,24} and one was a finite element²² analysis.
- Materials: two studies^{20,22} compared the glass ceramics IPS Empress (reinforced glass ceramic) and IPS e.max (lithium-disilicate) and the composite Paradigm MZ100 (zirconia reinforced composite) made by CAD/CAM system, one study²¹ compared the glass ceramics IPS Empress and IPS e.max and the composite Paradigm MZ100 and experimental blocks XR (fiber reinforced composite)made by CAD/CAM system, one study⁽²⁴⁾ compared Lava Ultimate™ (resin nano-ceramic) and composite Paradigm MZ100 also made by CAD/CAM, one study²³ used only IPS Empress by CAD/CAM, and one study⁽¹²⁾ compared IPS Empress and IPS e.max made with heat pressing.
- Cement: four studies^{12,20,21,23} cemented the restoration with adhesive resin cements, one study²⁴ cemented with self-adhesive resin cement and the finite element analysis study²² didn't include the cement as an interface.
- Preparation design: one study¹² compared four different preparation designs, occlusal preparation

with chamfer finish-line or straight-bevel finish-line with the preparation whichever totally in enamel or in dentin and the finish line in enamel.

- Restoration thickness: one study²⁴ compared three different thicknesses for the occlusal veneers 0.3, 0.6 and 1 mm.
- Cyclic loading: two studies^{20,21} made cyclic loading at 200N, followed by 400, 600, 800, 1000, 1200 and 1,400 N at a maximum of 30,000 cycles each, two studies^{12,23} made thermal cycling and mechanical loading in a masticatory simulator then loaded until fracture in a universal testing machine, one study²⁴ did not do cyclic loading and used a universal testing machine to subject the specimens to vertical load to fracture and the finite element analysis study²² did non-linear contact analysis to mimic occlusal loading at 200N and 800N.

3.2 Results

- Restoration thickness had no influence on the fracture resistance.
- The design of the finish-line had no effect on the fracture resistance.

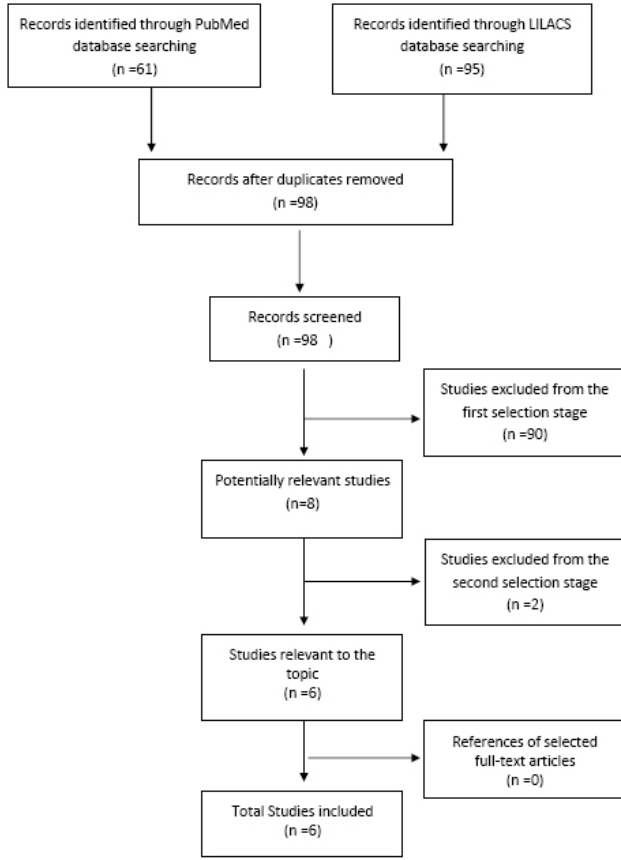


Figure 1. Schematic study selection procedure.

- Restoration material had an influence on the fatigue resistance: all of the studies^{12,20-22} that compared the glass ceramics IPS Empress with IPS e.max showed better fatigue resistance results for the e.max restorations, regarding the comparison between glass ceramics and composite²⁰⁻²², the composite showed better fatigue resistance, the study that compared resin nano-ceramic with composite²⁴ showed better fracture strength for the resin nano-ceramic.

4. Discussion

The benefits of decreasing retentive features of tooth preparations could be increased by the application of concepts used in treatment with anterior laminate veneers, hence the proposal for posterior “occlusal veneers” (thin onlay/overlay with non-retentive design). Such restorations could compete with gold onlays/overlays. Occlusal veneers are extra coronal restorations demanding a simple preparation lead by anatomical considerations and occlusal clearance²⁰.

The fracture resistance of all-ceramic restorations is subjective to several factors, such as composition and fatigue of the ceramics, technique of construction, the design of the preparation and cementing technique²⁵.

To simulate the clinical condition, the dynamic fatigue was assessed in a universal testing machine²⁶.

Occlusal veneers are a new restoration with no specific recommendation for the material that it can be made with, neither the preparation design nor the restoration thickness. So this systematic review aimed to evaluate the fatigue resistance of bonded posterior occlusal veneers made with different preparation designs, depths and materials.

Testing a ceramic’s fracture resistance in vitro is important before its clinical application. Static loading to fracture is a test widely used that can give an indication of whether a material and a type of restoration can be considered as viable clinical option. However, it can only show the strength of a restoration immediately after bonding and most likely it shows values of fracture resistance that are not indicative of the longevity of the restoration. In the mouth, restorations are loaded during their lifetime with millions of cycles which can cause a substantial reduction in the strength of the material as a result of fatigue^{27,28}. All ceramic restorations can be subjected to fatigue testing from 10,000 cycles to 1,200,000 cycles²⁹.

In complex multilayered restorations, such as cemented ceramic restorations, several factors contribute to the mechanical behavior of the restoration/tooth system. The intrinsic strength of each component of the system (i.e., tooth, adhesive system, luting cement, and restoration), the thickness of the restorative material, the ratios of modulus of elasticity between the restoration, the cement and dentin, and finally the quality of the adhesive interface between these layers in terms of bond strength³⁰.

The study¹² that measured the effect of different marginal preparation designs showed that it had no influence on the fracture resistance. The cause might be that the point where the load was applied during the test of fracture was away from the finish line. No other studies assessing the effect of the finish line on occlusal veneer-restorations were found in the literature. Therefore the choice of the finish-line can depend on the clinician’s choice based on the case.

The three studies²⁰⁻²² that compared occlusal veneers made of composite with those made of glass ceramics showed that the composite materials regarding restoration strength seem to consistently demonstrate more favorable

properties than their conventional ceramic counterparts. It seems that greater flexural strength does not necessarily result in a restoration with a greater load tolerance³¹. The IPS e.max has flexural strength of 256 MPa and IPS Empress of 127 MPa while the resin MZ100 has flexural strength of 150 MPa and these values were not reflected in their survival rates. This may be attributed to the fact that the failure caused by tensile stresses is affected by the ratios of the modulus of elasticity between the restoration and the cement and dentin more than it is affected by the intrinsic strength and the thickness of the material¹. The modulus of elasticity of composite resin is 16-20 MPa and that of dentin is 18.5 MPa which are very close and this maybe the reason for the good performance of the composite resin groups. Also the ceramics are brittle and they cannot withstand the high tensile stresses in the central groove³³. So, the energy was freed by means of cracks¹. Although there were no statistical differences between the composite resins tested (3M™ Paradigm™ MZ100 and XR), the absolute survival of all restorations in group XR can be caused by the enhancement of mechanical properties by the addition of fibers³⁴. Composite resin restorations are anticipated to preserve the antagonistic enamel but will wear more than the ceramics³⁵.

The study¹² that compared the 2 glass ceramics IPS e.max and IPS Empress made by heat pressing, the IPS e.max showed better results owing to their higher flexural strength.

The one study²⁴ that compared Lava Ultimate™ (resin nano-ceramic) with composite (3M™ Paradigm™ MZ100), showed that Lava Ultimate™ had significantly higher fracture strength than 3M™ Paradigm™ MZ 100, this may be due to the higher flexural strength of the resin nano-ceramic (204 MPa) compared to the composite blocks (150 MPa).

In one study²³, the occlusal veneers made of IPS Empress CAD developed surface cracks or fractures during thermal cycling and mechanical loading and therefore excluded from fracture strength testing. This was attributed to the tooth preparation design applied, which with the preparation of a finish line, could have resulted in generating stress bearing areas under the thin occlusal veneer at the cusp tips, as well as the relatively low flexural strength of IPS Empress.

5. Conclusions

In summary, the following conclusions can be drawn:

- Occlusal veneers were found to be a successful mean of restoring erosive or attrite posterior teeth regarding fatigue resistance.

- CAD/CAM composite resin and composite-ceramic overlays had higher fatigue resistance than the ceramic overlays.

6. Recommendations

Studies need to change at a fast pace from being predictable clinical trials to being more innovative in research ideas, such as additional chemical modification³⁶⁻⁴⁰ in the adhesives by addition of functional group monomers, bioactive particles and shock absorbent constituents. Since commonly the induced tensile stress surpasses the compressive stresses, strengthening must be added to deliver the required strength and ductility⁴¹. Using recent diagnostic tools to test the post-operative clinical performance is highly recommended⁴²⁻⁴⁵.

7. References

1. Kelly JR. Clinically relevant approach to failure testing of all-ceramic restorations. *J Prosthet Dent.* 1999 Jun; 81(6):652-61.
2. Rosenblum MA, Schulman A. A review all-ceramic restoration. *J Am Dent Assoc.* 1997 Mar; 128(3):297-307.
3. Van Dijken JW. All-ceramic restorations: classification and clinical evaluations. *Compend Contin Educ Dent.* 1999; 20(12):1115-24.
4. Felden A, Schmalz G, Federlin M, Hiller KA. Retrospective clinical investigation and survival analysis on ceramic inlays and partial ceramic crowns: Results up to 7 years. *Clin Oral Investig.* 1998 Dec; 2(4):161-7.
5. El-Mowafy O, Brochu JF. Longevity and clinical performance of IPS-empress ceramic restorations – A literature review. *J Can Dent Assoc.* 2002; 68(4):233-7.
6. Kramer N, Frankenberger R. Clinical performance of bonded leucite-reinforced glass ceramic inlays and onlays after eight years. *Dent Mater.* 2005 Mar; 21(3):262-71.
7. Otto T, De Nisco S. Computer-manufactured, direct ceramic restorations: A prospective, clinical 10-year study of Cerec CAD-CAM inlays and onlays. *Schweiz Monatsschr Zahnmed.* 2003; 113(2):156-69.
8. Attia A, Kern M. Influence of cyclic loading and luting agents on the fracture load of two all-ceramic crown systems. *J Prosthet Dent.* 2004 Dec; 92(6):551-66.
9. Heintze SD, Cavalleri A, Zellweger G, Buchler A, Zappini G. Fracture frequency of all-ceramic crowns during dynamic loading in a chewing simulator using different loading and luting protocols. *Dent Mater.* 2008 Oct; 24(10):1352-61.
10. Stappert CF, Att W, Gerds T, Strub JR. Fracture resistance of different partial-coverage ceramic molar restorations:

- An in vitro investigation. *J Am Dent Assoc.* 2006 Apr; 137(4):514–22.
11. Stoll R, Sieweke M, Pieper K, Stachniss V, Schulte A. Longevity of cast gold inlays and partial crowns. A retrospective study at a dental school clinic. *Clin Oral Investig.* 1999 Jun; 3(2):100–4.
 12. Clausen J-O, Abou Tara M, Kern M. Dynamic fatigue and fracture resistance of non-retentive all-ceramic full-coverage molar restorations. Influence of ceramic material and preparation design. *Dental Materials.* 2010 Jun; 26(6):533–8.
 13. Magne P, Belser U. Understanding the intact tooth and the biomimetic principle. In: Magne, Belser, editors. *Bonded Porcelain Restorations in the Anterior Dentition: A Biomimetic Approach.* Chicago: Quintessence Publishing Co; 2002. p. 23–55.
 14. Barron RP, Carmichael RP, Marcon MA, Sandor GKB. Dental erosion in gastro esophageal reflux disease. *J Can Dent Assoc.* 2003 Feb; 69(2):84–9.
 15. Lussi A, Hellwig E, Ganss C, Jaeggi T. Buonocore memorial lecture. *Dental Erosion: Oper Dent.* 2009 May-Jun; 34(3):251–62.
 16. Vailati F, Belser UC. Full-mouth adhesive rehabilitation of a severely eroded dentition: The three-step technique. Part 1. *Eur J Esthet Dent.* 2008; 3(1):30–44.
 17. Vailati F, Belser UC. Full-mouth adhesive rehabilitation of a severely eroded dentition: The three-step technique. Part 2. *Eur J Esthet Dent.* 2008; 3(2):128–46.
 18. Vailati F and Belser UC: Full-mouth adhesive rehabilitation of a severely eroded dentition: the three-step technique. Part 3. *Eur J Esthet Dent* 2008; 3(3):236–57.
 19. Moher D, Liberati A, Tetzlaff J, et al. Preferred reporting items for systematic reviews and meta-analyses: The PRISMA statement. *BMJ.* 2009 Jul; 339(b2535):332–6.
 20. Magne P, Schlichting LH, Maia HP, Baratieri LN. In vitro fatigue resistance of CAD/CAM composite resin and ceramic posterior occlusal veneers. *J Prosthet Dent.* 2010 Aug; 104(3):149–57.
 21. Schlichting LH, Maia HP, Baratieri LN, Magne P. Novel-design ultra-thin CAD/CAM composite resin and ceramic occlusal veneers for the treatment of severe dental erosion. *J Prosthet Dent.* 2011 Apr; 105(4):217–26.
 22. Magne P, Stanley K, Schlichting LH. Modeling of ultrathin occlusal veneers. *Dental Materials.* 2012 Jul; 28(7):777–82.
 23. Skouridou N, Pollington S, Rosentritt M, Tsiitrou E. Fracture strength of minimally prepared all-ceramic CEREC crowns after simulating 5 years of service. *Dental Materials.* 2013 Jun; 29(6):70–7.
 24. Johnson AC, Versluis A, Tantbirojn D, Ahuja S. Fracture strength of CAD/CAM composite and composite-ceramic occlusal veneers. *J Prosthodont Res.* 2014 Mar; 58(2):107–114.
 25. Kern M, Fechtig T, Strub JR. Influence of water storage and thermal cycling on the fracture strength of all-porcelain, resin-bonded fixed partial dentures. *J Prosthet Dent.* 1994 Mar; 71(3):251–6.
 26. Kern M, Strub JR, Lu X-Y. Wear of composite resin veneering materials in a dual-axis chewing simulator. *J Oral Rehabil.* 1999 May; 26(5):372–8.
 27. Sobrinho LC, Cattell MJ, Glover RH, Knowles JC. Investigation of the dry and wet fatigue properties of three all-ceramic crown systems. *Int J Prosthodont.* 1998 May-Jun; 11(3):255–62.
 28. Zahran M, El-Mowafy O, Tam L. Fracture strength and fatigue resistance of all-ceramic molar crowns manufactured with CAD/CAM technology. *J Prosthodont.* 2008 Jul; 17(5):370–7.
 29. Drummond JL. Ceramic behavior under different environmental and loading conditions. In: George E, Theodore E, William AB, Editors. *Dental Materials in vivo: Aging and Related Phenomena.* Quint Pub; 2003. p. 40.
 30. El-Damanhoury H, Haj-Ali RN, Platt JA. Fracture Resistance and microleakage of endocrowns utilizing three CAD-CAM blocks. *Oper Dent.* 2015 Mar-Apr; 40(2):201–10.
 31. Fennis WMM, Kuijs RH, Kreulen CM, Verdonschot N, Creugers NH. Fatigue resistance of teeth restored with cuspal coverage composite restorations. *Int J Prosthodont.* 2004 May-Jun; 17(3):313–7.
 32. Craig RG. Selected properties of dental composites. *J Dent Res.* 1979 May; 58(5):1544–50.
 33. Magne P, Belser UC. Porcelain versus composite inlays/onlays: Effects of mechanical loads on stress distribution, adhesion, and crown flexure. *Int J Periodontics Restorative Dent.* 2003 Dec; 23(6):543–55.
 34. Schlichting LH, Andrada MA, Vieira LC, de Oliveira Barra GM, Magne P. Composite resin reinforced with pre-tensioned glass fibers. Influence of prestressing on flexural properties. *Dent Mater.* 2010 Feb; 26(2):118–25.
 35. Kunzelmann KH, Jelen B, Mehl A, Hickel R. Wear evaluation of MZ100 compared to ceramic CAD/CAM materials. *Int J Comput Dent.* 2001 Jul; 4(3):171–84.
 36. Zahedi JAM, Ziaie F, Larijani MM, Borghei SM, Kamaliyanfar A. Synthesis and characterization of sodium-carbon apatite nano-crystals by chemical sedimentation method. *Indian J Sci Technol.* 2012 Mar; 5(S3):2464–7.
 37. Rastegari F, Rastegari F. Silicon nanocrystal memories. *Indian J Sci Technol.* 2012; 5(S3):2451–4.
 38. Bilankohi SM, Ebrahimzadeh M, Ghaffary T, Zeidiyam M. Scattering, absorption and extinction properties of Al/TiO₂ core/shell nano-spheres. *Indian J Sci Technol.* 2015 May; 8(S9):27–30.

39. Raj MS, Arkin VH, Jagannath AM. Nanocomposites based on polymer and hydroxyapatite for drug delivery application. *Indian J Sci Technol.* 2013 May; 6(S5):4653–8.
40. Prince MJA. Optimizing ultralow interfacial tension by altering surfactant concentration through emulsion test. *Indian J Sci Technol.* 2014 Nov; 7(S7):10–2.
41. Karthik Pandian SJ, Ramachandra Murthy A, Helen Santhi M. Investigations on RC beams retrofitted with UHSCC overlay under fatigue loading. *Indian J Sci Technol.* 2016 Feb; 9(5):1-5.
42. Lee SY, Lim SR, Cho YS. Remineralization effect of fluoride on early caries lesions using a Quantitative Light-Induced Fluorescence-Digital (QLF-D). *Indian J Sci Technol.* 2015 Jan; 8(S1):457–61.
43. Jalali T, Pooshimin R. Introduction of 3d photonic crystal waveguide structure by calculating effective refractive index. *Indian J Sci Technol.* 2015 May; 8(S9):20–6.
44. Park YW, Lim CH, Jung HR, Yang ON, Bbaek CM. Appropriate inspection distance of digital X-ray imaging equipment for diagnosis. *Indian J Sci Technol.* 2015 Apr; 8(S8):380–6.
45. Bharathi K, Karthikeyan S. A novel implementation of image segmentation for extracting abnormal images in medical image applications. *Indian J Sci Technol.* 2015 Apr; 8(S8):380–6.